

OPHTHALMOLOGIC APPARATUS

BACKGROUND OF THE INVENTION

Field of the Invention

5 The present invention relates to an ophthalmologic apparatus used in an ophthalmologic clinic and the like.

Related Background Art

In recent years, a large number of apparatuses
10 using image pickup elements have been developed.

Even in ophthalmologic image taking apparatuses,
ophthalmologic apparatuses in which an image of an
eye to be examined is obtained as an electronic image
using image pickup elements instead of a conventional
15 silver-halide film have been developed to conduct
electronic filing, a remote diagnosis, a diagnostic
support using a computer, and the like.

According to such an ophthalmologic apparatus,
for example, in the case of a non-mydriatic eye
20 fundus camera, focusing and alignment adjustment are
conducted using infrared light by a monochrome camera
at the time of observation. In addition, a still
image is picked up in synchronization with strobe
light using another color camera at the time of image
25 taking.

However, in recent years, an eye fundus camera
comes to be used which includes not respective

special image pickup elements for infrared observation and color still image taking which are used in a conventional apparatus but a common image pickup element.

5 When the common image pickup element is used for observation and image taking, a light source for observation using infrared light is different from a light source for color still image taking using strobe light. Therefore, in order to obtain suitable
10 images at the observation and the image taking, it is necessary to set respective different gains.

For example, as disclosed in Japanese Patent Application Laid-Open No. 04-038582, there has been a method in which a gain of a camera is increased at
15 the time of observation with low illumination to improve a contrast in an image and a gain of a camera is reduced at the time of image taking with high illumination to improve an S/N ratio of a taken image.

Thus, according to the above-mentioned
20 conventional example, the gain of the observation camera and the amount of light from the observation light source are adjusted to improve the contrast in the observation image. However, when the gain and the amount of light are simply changed, a contrast in
25 the entire image including an aperture region is enhanced. Therefore, it is impossible to enhance a contrast in only a region of interest such as a blood

vessel which becomes an index in focusing and alignment adjustment. Accordingly, a sufficient contrast cannot be obtained by only adjusting the gain and the amount of light, so that there is the 5 case where it is difficult to conduct focusing and alignment adjustment.

Fig. 4 is a histogram of the entire image in observation. The abscissa indicates brightness and the ordinate indicates a frequency. In Fig. 4, 10 brightness levels of an aperture region are distributed in a range "A", brightness levels of the entire eye fundus are distributed in a range "B", and brightness levels of blood vessels near an optic disk portion which are used for focusing and alignment 15 adjustment are distributed in a range "C".

When infrared light is used as observation light, the reflection from not a retina but a choroid becomes dominant, so that a range in which image data of the region of interest on the retina are 20 distributed is extremely narrow as shown in Fig. 4. Therefore, the contrast in the region of interest cannot be almost improved by only a linear correction such as the adjustment for the gain of the camera and the amount of observation light.

25 On the other hand, in the case of still image taking using strobe light, a correction method is desired which is different from a correction at the

time of observation such as a gamma correction for monitor or a linear gain correction. Therefore, in order to improve the contrast in the observation image, a special correction circuit for observation
5 is required as disclosed in Japanese Patent Application Laid-Open No. 05-199998. When such a special correction circuit is used, the entire circuit is upsized and complicated, thereby increasing a cost.

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SUMMARY OF THE INVENTION

An object of the present invention is to solve the above-mentioned problems and to provide an ophthalmologic apparatus capable of improving a
15 contract in a region of interest such as a blood vessel at observation without using a special correction circuit for observation.

In order to achieve the above-mentioned object, according to one aspect of the present invention, an
20 ophthalmologic apparatus includes: observation illumination means for illuminating an eye fundus of an eye to be examined in observation operation; image taking illumination means for illuminating the eye fundus in image taking operation; image pickup means
25 for electrically converting an image of the eye fundus obtained by both the illumination means into an image signal; conversion means for converting the

image signal obtained by the image pickup means into a digital value; a frame memory for storing the digital value data of the image signal; a rewritable lookup table; and rewrite means for rewriting the 5 data in the lookup table in synchronization with the observation operation and the image taking operation.

Further, according to another aspect of the present invention, an ophthalmologic apparatus includes: observation illumination means for 10 illuminating an eye fundus of an eye to be examined in observation operation; image taking illumination means for illuminating the eye fundus in image taking operation; image pickup means for electrically converting an image of the eye fundus obtained by 15 both the illumination means into an image signal; conversion means for converting the image signal obtained by the image pickup means into a digital value; a plurality of lookup tables for storing different data for correcting the digital value of 20 the image signal; and selection means for selecting a desired lookup table from the plurality of lookup tables in accordance with the observation operation and the image taking operation.

25 BRIEF DESCRIPTION OF THE DRAWINGS

Fig. 1 is a structural diagram of an eye fundus camera;

Fig. 2 is a graph of a lookup table (LUT) at the time of observation;

Fig. 3 is a graph of an LUT at the time of image taking operation; and

5 Fig. 4 is a histogram of image data in infrared observation.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

The present invention will be described in 10 detail based on an embodiment shown in the drawings.

Fig. 1 is a structural diagram of an eye fundus camera according to a first embodiment of the present invention.

In front of an eye to be examined E, an 15 objective lens 1 is disposed as an eye fundus observation and image taking optical system. On an optical path in the rear of the objective lens 1, a holed mirror 3 having an image taking diaphragm 2 in a hole portion, an image taking lens 4 a part of 20 which is moveable along the optical path for focusing, a half mirror 5, and an image pickup unit 6 such as a television camera are arranged in order.

In the light reflecting direction of the half mirror 5, a fixation light 7 conjugate with an eye 25 fundus Er is disposed to present a fixation target to the eye to be examined E. The fixation light 7 is composed of, for example, an LED array in which LEDs

are arranged in dot matrix, or a backlight made from LEDs or the like and a dot matrix liquid crystal shutter. Therefore, light transmission/non-transmission of a dot at an arbitrary position of a
5 two-dimensional matrix is controlled, so that the fixation target can be presented at the arbitrary position for the eye to be examined E. Note that an external fixation light is separated from the image taking optical system and used as the fixation light.

10 Also, in an illumination optical system located on a light incident side of the holed mirror 3, an observation light source 10 such as a halogen lamp for emitting visible light, a condenser lens 11, a visible cutting filter 12 for cutting off the visible
15 light, a strobe light source 13 for emitting a flash of visible light, a diaphragm 14 having a ring-shaped opening, an infrared cutting filter 15 for cutting off infrared light, and a lens 16 are arranged in order from the observation light source 10 side.

20 An output of the image pickup unit 6 is connected with a frame memory 21 and an LUT (lookup table) 22 through an A/D converting section 20. The frame memory 21 is connected with an LUT setting section 23 and the LUT 22. An output of the LUT 22
25 and an output of the LUT setting section 23 are connected with an image control section 24.

The image control section 24 is connected with

a D/A converting section 25, a recording medium 26, an information input unit 27, and a control circuit 28. An output of the D/A converting section 25 is connected with a monitor 29. The control circuit 28
5 is connected with a right-and-left-eye selection switch 30 and connected with the strobe light source 13 through a strobe light emission control circuit 31.

First, before image taking, a file format used in the case where patient information such as an ID
10 number, a name, a birth date, and a sex of a person to be examined and a taken image are outputted is inputted to the image control section 24 through the information input unit 27 by a photographer.
Subsequently, the objective lens 1 is located in the
15 front of the eye to be examined E and the observation light source 10 for eye fundus observation is turned on. Light from the observation light source 10 is condensed by the condenser lens 11. Visible light of the condensed light is cut off by the visible cutting
20 filter 12. Observation light considered to be infrared light passes through the strobe light source 13, the diaphragm 14, and the lens 16, is reflected to the left by a mirror portion of the holed mirror 3, and passes through the objective lens 1 to illuminate
25 the eye fundus Er through a pupil Ep of the eye to be examined E.

At this time, the infrared cutting filter 15 is

removed from the optical path by a mechanism which is not shown. Then, an image of the eye fundus illuminated with the observation light is again passed through the objective lens 1, the image taking 5 diaphragm 2 of the holed mirror 3, and the image taking lens 4, transmitted through the half mirror 5, and formed onto the image pickup unit 6.

The image pickup unit 6 which is sensitive to infrared light and visible light converts the 10 received eye fundus image into a video signal and then outputs the obtained video signal to the A/D converting section 20. The video signal which is inputted to the A/D converting section 20 is converted from analog data to digital data.
15 Observation image data corresponding to a frame of the image of the eye to be examined, which is converted into the digital data, is stored in the frame memory 21.

Next, the LUT setting section 23 extracts a 20 histogram from image data stored in the frame memory 21, produces an observation LUT for enhancing an image region such as a blood vessel on a retina with respect to ranges B and C as shown in Fig. 4, for example, the LUT as shown in Fig. 2, and sets the 25 observation LUT in the LUT 22.

Also, image data outputted from the A/D converting section 20 is inputted to the LUT 22,

subjected to gradation conversion by the LUT 22 which is set as described above, and then outputted to the D/A converting section 25. The D/A converting section 25 converts inputted digital data into an 5 analog signal and then outputs the analog signal to the monitor 29.

Thus, an observation image such as a blood vessel image in which a contrast in a region of interest is enhanced is displayed on the monitor 29.
10 While observing an eye fundus image displayed on the monitor 29, the photographer conducts precision alignment between the eye to be examined E and the image pickup unit, focusing, and checking of an image taking area. After it is ensured that the image 15 taking area, the alignment, and the focusing are preferable, the photographer operates an image taking switch which is not shown to conduct still image taking.

The control circuit 28 which has detected the 20 input by the image taking switch is adapted to insert the infrared cutting filter 15 onto the optical path and output an image taking start signal to the image control section 24. After that, the control circuit 28 waits a light emission timing signal for the 25 strobe light source 13 which is outputted from the image control section 24.

When the light emission timing signal for the

strobe light source 13 is received by the control circuit 28, the control circuit 28 sends a light emission signal to the strobe light emission control circuit 31 without delay, thereby emitting a light flux from the strobe light source 13. The light flux emitted from the strobe light source 13 passes through the objective lens 1 to illuminate the eye fundus Er of the eye to be examined E as in the case of the observation light. The eye fundus image is formed onto the image pickup surface of the image pickup unit 6, so that a video signal is outputted to the A/D converting section 20.

The image control section 24 synchronizes a video signal corresponding to a frame which is outputted from the image pickup unit 6 with strobe light emission. The video signal is converted into digital data by the A/D converting section 20 and then stored in the frame memory 21. Next, an LUT for still image taking, for example, an LUT for correcting a gamma characteristic of the monitor 29 as shown in Fig. 3 is produced in the LUT setting section 23 and is set in the LUT 22.

Subsequently, eye fundus image data stored in the frame memory 21 is read out and subjected to gradation conversion by the LUT 22. After that, the eye fundus image data is converted into an image format such as BMP or a set compression ratio to

convert the data into an image format such as JPEG, and the data is recorded on the recording medium 26 such as a MO or a hard disk.

If necessary, the image control section 24
5 reads out the image data from the frame memory 21. The image data is subjected to gradation conversion by the LUT 22, and then inputted to the D/A converting section 25 and outputted to the monitor 29. Therefore, the photographer can check the image.

10 When the A/D converting section 20, the frame memory 21, and the LUT 22 are provided as in this embodiment, it becomes possible to set an LUT for image correction after image taking. Accordingly, a period from image taking to image acquisition can be
15 shortened.

Note that, in this embodiment, when the LUT at the time of observation is produced, the region of interest is linearly enhanced using histogram data of the observation image. However, the present
20 invention is not limited to such an example. Histogram smoothing or the like can be conducted without using histogram data of an aperture region. In addition, when a level of the region of interest at the time of observation is predictable from the
25 gain of a camera, the amount of observation light, or the like, a previously fixed LUT may be used.

Also, the LUT for correcting the gamma

characteristic of the monitor 29 is used as the LUT for still image taking. However, the present invention is not limited to this. A linear LUT, an LUT for enhancing a macular portion and an optic disk portion, or the like may be used. Further, when a characteristic of a light source is changed, another LUT or the like may be used according to the characteristic of the light source. In addition, data written into an LUT can be changed.

10 Alternatively, the LUT 22 may have a plurality of LUTs. Data for observation is written into an LUT and data for image taking which is different from the data for observation is written into another LUT.

Note that, in the conventional example, the

15 data obtained by A/D conversion is stored in the frame memory and then subjected to gradation conversion by the LUT. However, the data obtained by A/D conversion may be subjected to gradation conversion by the LUT and then stored in the frame

20 memory.

A recording medium in which a program is stored according to this embodiment can be supplied to another system or apparatus. In this case, a computer in the system or apparatus can read out

25 program codes stored in the recording medium and execute the above-mentioned steps.

As described above, according to the

ophthalmologic apparatus in the present invention, optimum images can be easily obtained in observation and image taking without using the special correction circuit for observation.